

THE  
OSPOL  
WHITE  
BOOK

## A dental implant system unveiled



*Courtesy of Professor Per-Ingvar Brånemark*

## Preface

The picture above shows how bone tissue grows onto a titanium surface. You may recognize it. Professor Per-Ingvar Brånemark has used it in many of his lectures around the world.

We first met Professor Brånemark in December, 1985. The meeting changed our lives in more ways than one.

First and foremost, he led us to fascinating careers introducing a therapy that would forever change the nature of dentistry – and improve the quality of life of millions of patients.

Professor Brånemark also made us realize that no matter how well implant hardware is designed, it will always be secondary to the competence, dexterity and experience of the dentist using it.

Finally, he taught us the importance of balancing our business ambitions with a strong sense of integrity and respect: Respect for the patient, for nature and biology, and for Hippocrates' oath.

At Ospol, the harmony between living tissue and titanium symbolizes our commitment to this important balance. Some 20 years later, we now have a chance to show Professor Brånemark that his philosophy remains our guiding light.



*Hans Berglund,  
Göran Urde, Lennart Carlsson  
– founders of Ospol*

## Ospol's vision

We strive to give every person who needs to replace missing teeth access to professional treatment with dental implants.

Our contribution to such a development is to make implant technology easier to use, manage and provide. By becoming a preferred therapy among more dentists, implants will become more accessible to more patients.

## Ospol's business mission

Everything we do is aimed at accommodating our customers in their dual roles as clinicians and businesspeople. We will provide a modern implant system with excellent clinical performance. To this we add unique business tools and support that will benefit each dentist and each patient.

The work in our company is geared at enhancing our customers' ability to treat patients and run an effective practice. Their success is a prerequisite for our own success, and we view them as partners rather than customers. We share the same goal – to successfully treat more patients with dental implants.

By providing business tools and support, we wish to invest in dentists whose ambition is to develop the implant treatment aspect of their practice, with Ospol as their partner.

## Ospol's quality policy

- Ospol will always deliver products that fulfil legal and regulatory requirements, regardless of sales channel.
- Our products will have an error incidence that is so low as to not be disruptive to dentists or patients.
- All Ospol employees will work continuously to improve quality in all processes, in order to bring error incidence as close to zero as possible.
- Ospol will aim to keep promised delivery dates and will implement systems to avoid delays.
- In order to fulfil this quality policy, Ospol will inform and educate all employees. The company operates with preventive improvement of all internal processes, and all employees are evaluated frequently against established quality goals.
- Everyone in the Ospol organization is encouraged to suggest quality improvements or new measurements of quality goals. The CEO is responsible for evaluating, prioritizing and implementing these suggestions.

## Why we wrote this whitebook.

This is not a whitebook in the academic sense of the word. Its aim is not to provide exhaustive scientific documentation of our implant system, based on lengthy studies establishing every aspect of its effectiveness and safety.

The reason is simple: these studies have already been completed by others and, as such, are abundantly documented.

Over the years, the groundbreaking work by Professor Per-Ingvar Brånemark and his co-workers has been validated in thousands of scientific papers demonstrating the reliability of the therapy.

The true biological mechanisms behind osseointegration may still be unknown in part. Yet a predictable outcome can be achieved by following a well-documented protocol that covers aspects like the surgical procedure, the design of the implant hardware, and the material used to manufacture it.

In other words, the quality of the treatment has come to rely on common and accepted knowledge and science. If an implant system uses a well-known design and material composition, and is loaded according to known and accepted principles, it can be expected to behave clinically in a certain predictable way.

Even the FDA concurs that as long as the implant hardware conforms to specific basic requirements, companies can refer to “substantial equivalence” for obtaining registration:

*“FDA believes that special controls, when combined with the general controls, will be sufficient to provide reasonable assurance of the safety and effectiveness of a root-formed endosseous dental implant or endosseous dental implant abutment device. Thus, a manufacturer who intends to market a device of either of these generic types should<sup>1</sup> conform to general controls of the Federal Food, Drug and Cosmetic Act (the Act), including the premarket notification requirements described in 21 CFR 807, Subpart E;<sup>2</sup> address the specific risk to health associated with root-formed endosseous dental implants or endosseous dental implant abutment devices identified in this guidance; and<sup>3</sup> obtain substantial equivalence determination from FDA prior to marketing the device”.*

Quote from the FDA document: *Guidance for Industry and FDA Staff*

With the Ospan Implant System, we are claiming such equivalence (based on specific FDA and CE guidelines for substantial equivalency) for a long list of previously validated features and properties. The clinical documentation of these “generic” features and properties is readily available from a myriad of scientific sources.

To assist anyone interested in penetrating that documentation – as it pertains to the Ospan system – we have identified and compiled a great number of papers. Rather than reprinting the complete content in each instance, we summarize it in this whitebook. We also provide detailed information about each source, and how to access it on the Internet.

## Why we divided it into two parts.

The Ospan Implant System is presented in two sections of this whitebook. In the first section, we review existing documentation of those “generic” features of the system hardware for which we claim “substantial equivalence.”

Hence, Part One covers macro-design aspects such as the overall implant design and the conical abutment connection.

We also discuss factors influencing the implant behavior in bone – for example the roughness and oxidization of the surface.

All in all, Part One summarizes 112 scientific papers documenting these and other key properties of the Ospan Implant System.

In Part Two, we introduce a number of proprietary features of the system based on the clinical demands on a modern implant system. These are innovations (some of which are patented) developed by our team of implant designers. Though new in the context of implant design, these innovations are in no way entering uncharted biological territory. They all rest firmly on well-known mechanical principles. For example:

To improve primary stability, we have combined the advantages of a cylindrical screw and a conical core. To optimize the bone fill around the implants, we have improved their cutting properties. To secure stability in marginal bone, we have threaded the implants all the way to the top. To give the joint between implant and abutment optimal stability, we have made it conical.

And to facilitate early bone apposition by biomechanical bonding, we’ve oxidized the titanium surface with calcium, a Bioactive Surface Chemistry in accordance with Dr Y-T Sul’s thesis “The role of microporous structure and chemical composition of the surface oxide in enhanced osseointegration”.<sup>99</sup>

Because they are new, the clinical documentation of these enhancements is not as extensive as for the generic features. They have all, however, undergone either thorough mechanical testing, independent benchmarks against other systems, or pre-clinical studies performed on animals.

Part Two presents these tests, benchmarks and studies in detail.

We trust this will give implant dentists the confidence they need to use the Ospan system for improving the quality of life of their patients.

Our whitebook is founded on three simple but important principles:

1. The content reflects our commitment to honesty, completeness and transparency.
2. All validation of product effectiveness is based on accepted science, regulatory requirements and benchmarking of specific features.
3. Future clinical results will be continuously monitored through the process of post market clinical follow-up. Just like other modern implant systems, ours has all the proven characteristics you’d expect.

Part I.  
IMPLANT DESIGN  
CONICAL ABUTMENT CONNECTION  
TITANIUM IN BONE

## Generic features of the Ospot system

As we learn more about the unique biological inter-relationship of the dental implant restoration and the surrounding hard and soft tissues, implant dentistry steadily evolves. Nevertheless, if you scan clinical reports published in the major scientific journals, it quickly becomes clear that most of them deal with screw-shaped titanium implants – implants that are essentially similar to the Ospot Implant System.

The original Brånemark implant system has, for many years, shown safe and highly predictable clinical results for all indications. And implant systems that are substantially equivalent to the Ospot System have been proven in study after study to be at least as successful as the Brånemark System<sup>®\*</sup>. The conclusion can therefore safely be drawn that the Ospot Implant System can be expected to exceed acceptable success rates – as defined by Albrektsson, et al in 1981 & 1986,<sup>3,4</sup> consistently.

Indeed, guidelines provided by the FDA give manufacturers of dental implant devices an opportunity to submit simplified premarket notification processes if the products can provide logical reference to predicate devices. The same principle of equivalency exists for achieving CE certification. The generic features of our system for which we claim “substantial equivalence” are described on the pages of this section followed by a review of the existing documentation of those features.

\* More information can be found in the following references: 9, 10,11, 17, 20, 22, 24, 28, 30, 57, 58, 63, 65, 68, 69, 70, 71, 82, 89, 94, 95, 110.

# IMPLANT DESIGN

## 1. Screw shape

The Ospot implant is screw shaped, which is by far the most common macro-shape for dental implants. It is threaded for mechanical stability during the sensitive initial healing phase, and the additional surface area provided by the threads increases the bone to titanium interface. This has been shown to be critical to long-term osseointegration.

## 2. Tapered body

The core of the Ospot implant is slightly tapered, while the outer threaded profile is cylindrical. This shape combines the ease of surgical placement typical of a cylindrical implant body with the higher mechanical stability of a tapered implant.

## 3. Self-tapping

The Ospot implant is self-tapping. It cuts into the bone and creates threads as it is inserted, thus preserving bone mass and optimizing bone fill of the threads, which improves mechanical stability and speeds up the osseointegration process.

## 4. Threads in marginal bone

The Ospot implant has a threaded shoulderless neck. In early screw designs, the neck was frequently countersunk into marginal bone. Countersunk implants often showed marginal bone loss to the first thread. Furthermore, in modern screw-type implants it has been proven that a threaded neck provides greater mechanical stability



### Substantial equivalency

**Ospot's screw-shaped implant, with its self-tapping feature and shoulderless, threaded neck is substantially equivalent to systems designed by Nobel Biocare, Straumann®, 3i® and Astra Tech.**

### What does the documentation say?

#### 1. About the screw shape

Proven to be safe and effective in numerous studies over the last 20 years, the screw shape is one of the most well-documented implant features. For example a study that spanned over 20 years on the screw-shaped Brånemark System® implants showed a 98.9% success rate<sup>24</sup>. And in an 8-year study of non-submerged ITI implants, screw-shaped implants showed a better cumulative success rate than hollow cylinder implants.<sup>18</sup>

#### 2. About the tapered/cone-shaped body

A tapered/cone-shaped implant has proven to be highly successful even in early load situations.<sup>67</sup>

In another study, a slightly tapered implant and modified implant surface texture, anodized Cp Titanium, was shown to be a successful treatment alternative even in soft bone.<sup>40</sup>

Finally, the MkIV tapered Brånemark System® implant showed significantly higher resonance frequency value than standard cylindrical implants, indicating a higher interfacial stiffness at the implant-bone interface.<sup>81</sup>

#### 3. About self tapping

In a prospective longitudinal multicenter study, excellent 1-year clinical results of 95.6% were shown after placement and restoration of Brånemark System® self-tapping implants using a one-step protocol in completely and partially edentulous patients. All implants were stable after placement.<sup>12</sup>

Another prospective multicenter study showed that self-tapping implants were easier to place.<sup>22</sup> And in a study of the influence of implant design and of overload on marginal bone loss and implant success in the Brånemark System®, standard implants clearly showed a higher failure rate than self-tapping implants, both before and after loading.<sup>83</sup>

#### 4. About threads in marginal bone

In a study comparing marginal bone reaction to Astra Tech and Brånemark System® implants, the initial bone resorption was less for the Astra Tech implants compared to Brånemark System®.<sup>26</sup> Astra Tech implants feature a threaded neck.

In addition, an axisymmetric finite element analysis showed that a conical implant-abutment interface at the level of the marginal bone (combined with a threaded implant neck, sufficient implant wall thickness and modulus of elasticity) caused bone stresses resulting from axial load to occur lower down in bone. This minimizes the risk of marginal bone resorption due to accumulated microdamage in the bone.<sup>47, 48, 49</sup>

## CONICAL ABUTMENT CONNECTION

The Ospot system features an internal conical abutment connection with a separate center screw for cemented prosthetic restorations. From an engineering perspective, the cone form is one of the most stable mechanical connections between two parts. It also provides a tight seal and minimizes stress in marginal bone by distributing load.



### Substantial equivalency

Ospot's conical abutment connection is substantially equivalent to systems designed by Astra Tech, Straumann® and Ankylos®, all of which have been proven in clinical studies to offer good mechanical stability. As compared to flat-to-flat connections, conical abutment connections have also been proven to limit bacterial leakage and to minimize stress in marginal bone. The latter is hypothesized to lower the risk of stress-induced bone resorption.

### What does the documentation say?

#### 1. About mechanical strength

The shape of an interface between components in the abutment connection greatly impacts the stability of that connection. In theory, an implant with a conical interface can resist larger axial and transversal loads than an implant with a flat interface.<sup>47, 50</sup>

Bridge performance is also closely related to load transmission both at the bone-to-implant interface and between components within the implant-abutment-bridge cylinder complex. An internal conical interface demonstrated increased resistance to bending moments at the fixture-abutment interface compared to flat-to-flat butt joint interfaces.<sup>78</sup>

#### 2. About the biological seal

It has been shown that micro leakage can occur at the abutment-implant interface in osseointegrated implants and may cause malodor and inflammation of peri-implant tissues.<sup>44</sup>

A tight seal at the fixture-abutment interface has resulted in the maintenance of marginal bone around single tooth titanium implants.<sup>78</sup>

#### 3. About load distribution

The design of the implant-abutment interface has a profound effect upon the stress state in the marginal bone: It has been shown that anchorage strength is maximized if an implant is designed in a way that minimizes peak bone stress (as is the case with a conical abutment connection). This facilitates obtaining a marginal bone level close to the crest of the implant.<sup>47</sup>

In addition, an axisymmetric finite element analysis demonstrated benefits associated with a conical implant-abutment interface at the level of the marginal bone in combination with a threaded implant neck and suitable values of implant wall thickness and modulus of elasticity. The analysis showed that the peak bone stresses resulting from axial load arose deeper down in the bone thus minimizing the risk of marginal bone resorption due to accumulated microdamage.<sup>48, 49, 50</sup>

# TITANIUM IN BONE

## 1. Surface roughness

There is evidence that the surface structure of the implant is of importance to successful osseointegration. Moderately rough surfaces such as those of the Ospol implant have proven to be better for osseointegration than the machined surfaces of the original screw-shaped implants.

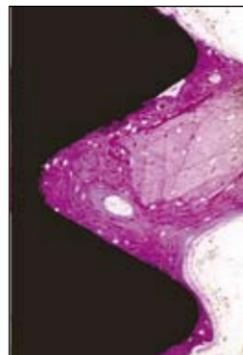
On the other hand, extreme surfaces roughness, such as occurs with etched or plasma sprayed, have an increased incidence of peri-implantitis because of the increased risk of retaining bacteria if exposed.

## 2. Anodization

Surface roughness can be achieved with etching, blasting, plasma spraying or anodization. All of these methods are well documented, widely used and considered safe. The Ospol Implant System's surface is first machined, and then anodized.

## 3. Commercially pure titanium grade 4

The Ospol Implant System is made of commercially pure titanium grade 4 (Cp Ti grade 4). Cp Ti grade 4 is stronger than commercially pure titanium grade 1 (Cp Ti grade 1) used in the original Brånemark implants. There is, however, no evidence in the literature that points to differences in osseointegration for the different grades of titanium.



### Substantial equivalency

**Ospol's surface texture is substantially equivalent to the surface of TiUnite® and is achieved using a process that is substantially equivalent to the process used for that system.**

### What does the documentation say?

#### 1. About surface roughness

In a review focusing on topographic and chemical properties of different surfaces, moderately rough surfaces showed stronger bone responses than smoother or rougher surfaces.<sup>7, 8</sup>

#### 2. About anodization

Surface roughness and enlargement are greater for oxidized implants than for turned implants. This results in significantly higher bone-to-implant contact as well as more bone in the threads. A histologic evaluation demonstrated a significantly higher bone response for anodic oxidized titanium implants than for implants with turned surfaces.<sup>55</sup> In another multicenter study, a total of 478 TiUnite® implants were followed of which 357 were placed in the maxillae. The one-year result showed a cumulative survival rate of 98.9%.<sup>34</sup>

#### 3. About Cp Ti grade 4

In a retrospective multicenter analysis of 3i® endosseous dental implants placed over 5 years in edentulous and partially edentulous jaws using 3i® Cp Ti grade 4 threaded and cylindrical implants, the success rate was 97.0% in the mandible and 93.8% in the maxillae.<sup>68</sup>

## Part 2.

**PRIMARY STABILITY**  
**STABLE AND TIGHT ABUTMENT CONNECTION**  
**MODERN IMPLANT SURFACE**  
**COMPACT FLEXIBLE SYSTEM**

## Special features of the Ospol Implant System

When we set out to create the design specifications for the Ospol Implant System, we began by examining current trends in implant dentistry and talking to active implant clinicians. We looked at smart solutions already in use and at areas that called for improvements. The messages we received from potential customers provided a clear direction for our design process, and the Ospol design team has focused on a limited number of important features.

These clinical requirements are defined on the pages of this section. Each definition is followed by a detailed explanation of the Ospol technical solutions and, when appropriate, there is information about how we have tested our solutions.

# PRIMARY STABILITY

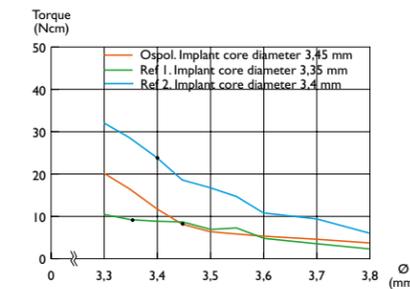
The ability to achieve optimal stability at the time of surgery in different quality and quantity of bone.

The Ospol implant is designed to provide optimal primary stability (mechanical stability). Excellent self-cutting properties make it possible to dimension the osteotomy with the same diameter as the core of the implant for maximum bone fill in the threads. In order to use the dense marginal bone for stability, the implant is threaded all the way to the top and the core has a slight cone shape.

## I. Self-tapping feature

Today, a cutting edge is commonly placed at the tip of the implant so it can cut threads as it is installed in the prepared site. Mechanical stability is achieved through the balance between compression of the bone and the amount of bone in the threads.

The challenge, however, lies in cutting complete threads without using excessive torque. One way of reducing the torque requirement is to prepare a site that is larger in diameter than the core of the implant. This will, however, reduce mechanical stability and leave open spaces in the threads. Ospol's solution is to optimize the cutting properties of the implant resulting in lowered torque and increased bone fill. The closer the diameter of the last cutting drill is to the core diameter of the implant, the more bone fill in the threads, which has a direct effect on mechanical stability. Our design team has been able to take advantage of the latest developments in machining techniques and has added geometry to the implant that was not possible to produce even a few years ago.



Graph comparing Ospol and competitors, showing threading torque for various drill diameters in a homogenous material. Dots show actual implant core diameter.

## 2. Conical implant core

In the upper third of the implant, the core has been made slightly conical. This means that the threads become gradually shallower. This design was chosen to improve stability by using the often denser bone quality in the marginal area. This design gives the desired stability effect without complicating the drilling and placement process as is the case with truly conical implants.



## STABLE, TIGHT IMPLANT/ ABUTMENT CONNECTION

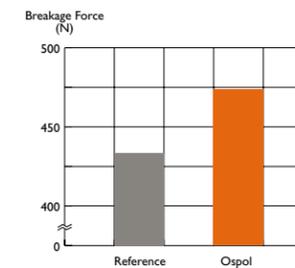
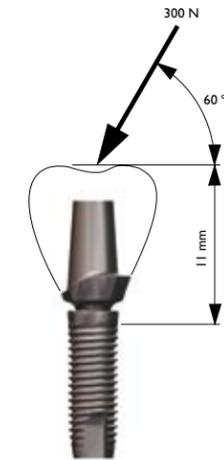
The ability to create a connection that is stable over time and tight enough to limit micro leakage.

The Ospol system is designed with a 17-degree internal cone connection between the implant and the abutment. An internal octagon in the implant has a dual purpose – to transfer torque during implant placement and as an indexing system when the abutments are used for single tooth replacements. The design of the abutment screw is “one-size-fits-all.” With its long shaft and low friction coating, it delivers optimal pre-load with a minimum of torque.

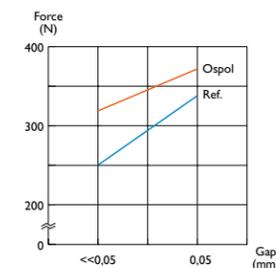
### Conical internal connection

Bending is the most unfavourable load for an implant and the most frequent cause of implant fracture. When a flat-to-flat interface, such as the original Brånemark external hex, is subjected to bending, more load is placed on the center screw than is the case with a conical abutment interface. A conical abutment also provides a tighter seal with less microleakage than a flat-to-flat abutment.

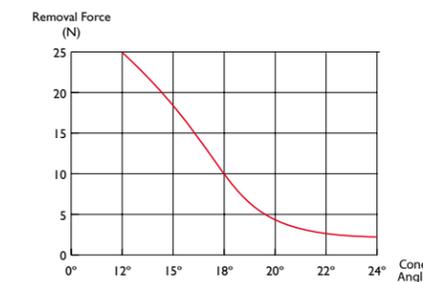
With a conical abutment, the amount of load placed on the center screw depends on the angle of the cone. The more aggressive the angle, the less the load on the screw. On the other hand, an aggressive angle causes locking between the parts, which makes separating the components difficult.



Load test comparison between Ospol and competitor implant indicating load force at breakage.



Comparison between Ospol and competitor showing applied load force (according to ISO/DIS 14801) in relation to gap width between abutment and implant.



Graph showing abutment removal force in relation to different cone angles.

**Special abutment removal tool**

The Ospol Implant System includes a specially designed tool for dismantling components. We have, therefore, been able to select an optimal angle with regards to loading and microleakage, while maintaining easy abutment removal.



**Impression-taking technique**

Conical interfaces demand much greater precision in the impression chain to achieve the same repeatability in height position as a flat-to-flat system, although repeatability is better for a conical system in every other direction. This is a problem shared by all implant systems with conical interfaces.

The Ospol Implant System however uses a conical/flat-surface combination, which means that height information for the implant and the implant replica uses a flat reference surface rather than the conical portion. This, in combination with modern machining technology, minimizes the problem of precision.

**Abutment screw design**

To prevent loosening, screws must be tightened properly. When a screw is tightened, it becomes elongated and the material supporting it is compressed. This happens as a result of torque being converted to longitudinal force by the pitch of the screw threads. Elongation of the screw is necessary to achieve a screw joint that will maintain its tension over time when its parts are subject to micromovement.



**LONG SCREW STEM**

In addition, the longer a screw is to begin with, the longer it becomes when a given force is applied and the better the ability of the screw joint to maintain force over time. The Ospol abutment screw has therefore been designed to be as long as possible. (See the table below.)

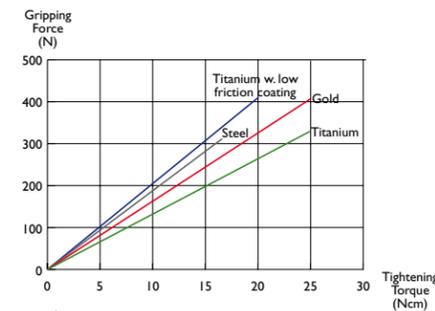
**LOW-FRICTION COATING**

When designing a screw, the selection of material is critical to maintaining the tension in the screw joint. Titanium is a highly appropriate material because it stretches more than, for example, steel, when a given force is applied.



The drawback of titanium compared to steel or gold is, however, that titanium has higher friction. The coefficient of friction between two titanium parts may be as high as 0.5, while the comparable value for steel is approximately 0.1.

High friction can in part be compensated for by higher torque, but increasing torque is not ideal because it increases torsion stress in the screw stem. Instead, the Ospol Implant System is treated to reduce friction.



Graph of abutment screws of different materials and coatings showing the Ospol material and coating choice gives a higher gripping force at less tightening torque.

## MODERN SURFACE

Calcium-oxidized commercially pure titanium surface, to facilitate early bone apposition.

The Ospot Implant System features a patented calcium-deposited, oxidized titanium surface, which is in accordance with the results of Dr Young-Taeg Suls research. The Ospot implant surface consists of a thin layer of micro porous titanium oxide saturated with 11% calcium that will optimize the tissue response.

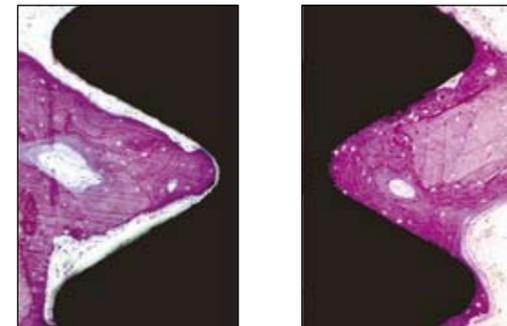
### Thesis of Dr Young-Taeg Sul

On Bone Tissue Response To Oxidized Titanium Implants  
 “The role of micro-porous structure and chemical composition of the surface oxide in enhanced osseointegration”

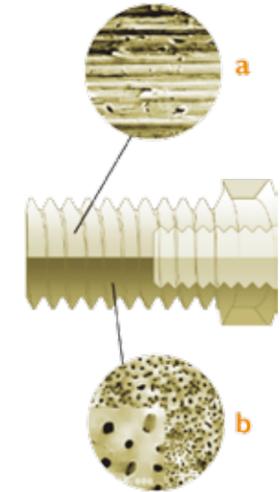
Dept of Biomaterial Sciences / Handicap Research, Institute for Surgical Sciences, Faculty of Medicine, University of Gothenburg, Sweden Gothenburg 2002 (99)

Dr Sul used clinical screw type oral implants of 18 mm in length and a diameter of 3.75 mm for his in vivo studies. One side of the implant (the control) had a non-modified, turned surface, and the other side of the same implants had an electrochemical calcium deposited oxidized surface.

Dr Sul showed a possible reinforcement of osseointegration by mechanical interlocking and a possible chemical bonding between bone and implant surface. Mechanical interlocking is associated with the surface roughness or pore configurations, while chemical bonding is dependent on surface chemistry.

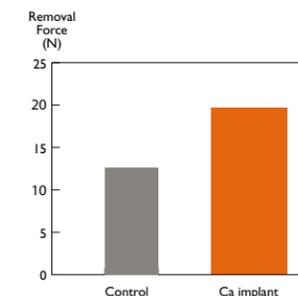


Histology showed that the control had less bone in close contact to the implant surface, compared to the Ca Implant.

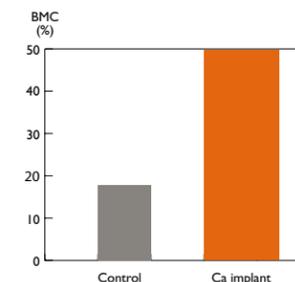


SEM pictures showing a typical turned machined (control) implant surface compared to the thin layer of microporous titanium oxide saturated with calcium on the calcium implant (Ca implant).

In Dr Sul’s study, oxidized microporous implants showed significantly stronger bone response as compared to nonporous machined implants. Calcium deposited, oxidized titanium implants showed that osteoconductivity was more pronounced and thus generated a faster, stronger osseointegration as compared to machined implants and other oxidized surfaces tested.



The Ca implant also demonstrates a highly significant early increase of mean removal torque values (Ncm) compared to the control (machined surface).



Calcium deposited, oxidized microporous titanium implants showed significantly improved bone response as compared to machined (control) and other oxidized titanium implants. An in vivo study of Ca implants demonstrated a highly significant increase of the mean BMC (Bone to Metal Contact) value after a 6-week follow up as compared to the control.

## COMPACT SYSTEM WITH MINIMAL COMPONENTS

The ability to treat many indications with few components.

The Ospot 85+ series has around 50 components total and, according to our reference group of active clinicians, those components will cover at least 85% of the clinical situations in a normal implant practice. The following technical solutions contribute to make the Ospot system compact and easy to handle.

### Focus on cemented solutions

Because of the simpler protocol associated with cementing for single tooth and short partial bridge indications, cementation is the most common restorative solution. For full mouth reconstructions, Ospot recommends the Procera® Bridge Adapter, which will allow a traditional screw-retained treatment protocol.

### One-size abutment screw

The interior design of each Ospot abutment is altered to accommodate a single size of abutment screw. The retention properties of the abutment screw are largely dependent on the length of the “stem.” Thus, using one screw size regardless of the length of the abutment keeps performance consistent.

### Efficient screwdriver system

Because the same screwdriver is used for cover screws, healing abutments, abutment screws and the guide-pin for the impression coping, the Ospot system has a low number of different screwdrivers. In addition, the implant inserter incorporates a friction grip tip for picking up and placing cover screws and healing abutments without changing the machine tool.

### A single abutment design for all indications

The entire range of Ospot abutments is equipped with the same octagonal design for correctly indexing the abutment in the implant. Consequently all abutment designs can be used for single tooth replacements as well as all other indications.

### Unique packaging and storage solution

A streamlined packaging and in-practice storage solution also help keep the Ospot system compact. All Ospot products come packed in a unique container that will simplify storage and handling. And the implants themselves are enclosed in a double-barrier cylinder that can be easily transferred to the surgical tray. The product containers are organized in a binder storage solution that holds up to 42 individual containers.



# List of references

This is a list of some of the most relevant articles, studies and text books on modern dental implantology including those referenced in this whitebook.

Abstracts on most of these can be found on internet at the following addresses: [www.pubmed.com](http://www.pubmed.com), [www.medline.cos.com](http://www.medline.cos.com), [www.embase.com](http://www.embase.com)  
You can also find links to these sources at our website [www.ospol.com](http://www.ospol.com)

Brånemark P-I, Zarb T, Albrektsson T. Tissue-Integrated Prosthesis – Osseointegration in Clinical Dentistry. Quintessence Publ. Co. Inc, Chicago, USA (1985)

Brånemark P-I, Chien S, Gröndahl H-G, Robinson K. The Osseointegration Book; From Calvarium To Calcaneus. Quintessenz Verlags-GmbH, Berlin, Germany (2005)

1. Adell R, Lekholm U, Rockler B, Brånemark P-I. A 15-year study of osseointegrated implants in treatment of totally edentulous jaws. *Int J Oral Surg* 1981;6:387-416.
2. Adell R, Eriksson B, Lekholm U, Brånemark P-I, Jemt T. A long term follow-up study of osseointegrated implants in the treatment of totally edentulous jaws. *Int J Oral Maxillofac Implants* 1990;5:347-359.
3. Albrektsson T, Brånemark PI, Hanson HA, Lindström J. Osseointegrated titanium implants. Requirements for ensuring a long lasting , direct bone-to-implant anchorage in man. *Acta Ortho Scand* 1981;55:155-170.
4. Albrektsson T, Zarb G, Worthington P, Eriksson RA. The long-term efficacy of currently used dental implants: A review and proposed criteria of success. *Int J Oral Maxillofac Implants* 1986;1:111-25.
5. Albrektsson T, Sennerby L. State of the art in oral implants. *J Clin Periodontol* 1991;18:474-481.
6. Albrektsson T, Johansson C, Lundgren AK, Sul Y, Gottlow J. Experimental studies on oxidized implants. A histomorphometrical and biomechanical analysis. *Appl Osseointegration Res* 2001;1:21-24.
7. Albrektsson T, Wennerberg A. Oral implant surfaces: Part 1-Review focusing on topographic and chemical properties of different surfaces and in vivo response to them. *Int J Prosthodont* 2004;17:536-543.
8. Albrektsson T, Wennerberg A. Oral implant surfaces: Part 1-Review focusing on clinical knowledge of different surfaces. *Int J Prosthodont* 2004;17:544-564.
9. Andersson B, Odman P, Lindvall AM, Branemark PI. Cemented single crowns on osseo-integrated implants after 5 years: results from a prospective study on CeraOne. *Int J Prosthodont* 1998;11(3):212-218.
10. Arvidson K, Bystedt H, Frykholm A, von Konow L, Lothigius E. Five-year prospective follow-up report of the Astra Tech Dental Implant System in the treatment of edentulous mandibles. *Clin Oral Implants Res.* 1998 Aug;9(4):225-34.
11. Arvidson K, Bystedt H, Frykholm A, von Konow L, Lothigius E. Five-year prospective follow-up report of the Astra Tech Dental Implant System for restoration of edentulous upper jaws. *J Dent Res* 1996;75:349.
12. Becker W, Becker BE, Israelsson H. One-step surgical placement of Brånemark Implants: A prospective clinical multicenter study. *Int J Oral Maxillofac Implants.* 1997;15:454-462.
13. Becker W, Becker BE, Ricci A, et al. A prospective multicenter clinical trial comparing one- and two-stage titanium screw-shaped fixtures with one-stage plasma-sprayed solid-screw fixtures. *Clin Implant Dent Relat Res* 2000;2:159-165.
14. Berglund T, Persson L, Klinge B. A systematic review of the incidence of biological and technical complications in implant dentistry reported in prospective longitudinal studies of at least 5 years. *J Clin Periodontol* 2002;29:197-212.
15. Berglundh T, Gislason O, Lekholm U, Sennerby L, Lindhe J. Histopathological observations of human periimplantitis lesions. *J Clin Periodontol.* 2004 May;31(5):341-7.
16. Binon PP. Implants and components: Entering the new millennium. *Int J Oral Maxillofac Implants* 2000;15:76-94.
17. Brocard D, Barthet P, Baysse E, Duffort JF, Eller P, Justumus P, Marin P, Oscaby F, Simonet T, Benque E, Brunel G. A multicenter report on 1,022 consecutively placed ITI implants: a 7-year longitudinal study. *Int J Oral Maxillofac Implants.* 2000;15(5):691-700.

18. Buser D, Mericske-Stern R, Bernard JP, Behneke A, Behneke N, Hirt HP, Belsler UC, Lang NP. Long-term evaluation of non-submerged ITI implants. Part 1: 8-year life table analysis of a prospective multi-center study with 2359 implants. *Clin Oral Implants Res.* 1997;8(3):161-172.
19. Callan D, Hahn J, Hebel K et al. Retrospective multicenter study of an anodized, tapered, diminishing thread implant: Success rate at exposure. *Implant Dentistry Vol* 9;4:329-333.
20. Chee W, Felton DA, Johnson PF, Sullivan DY. Cemented versus screw-retained implant prostheses: which is better? *Int J Oral Maxillofac Implants* 1999 Jan-Feb;14(1):137-141.
21. Collaert B, De Bruyn H. *Clin Oral Implants Res.* 1998 Apr;9(2):131-5  
Comparison of Brånemark fixture integration and short-term survival using one-stage or two-stage surgery in completely and partially edentulous mandibles.
22. Davarpanah M, Martinez H, Tecucianu JF, Alcoforado G, Etienne D, Celletti R. The self-tapping and ICE 3<sup>®</sup> implants: a prospective 3-year multicenter evaluation. *Int J Oral Maxillofac Implants* 2001;16(1):52-60.
23. Eckert SE, Wollan PC. Retrospective review of 1170 endosseous implants placed in partially edentulous jaws. *J Prosthet Dent* 1998 Apr;79(4):415-21.
24. Ekelund JA, Lindquist LW, Carlsson GE, Jemt T. Implant Treatment in the edentulous mandible: A prospective study on Brånemark system implants over more than 20 years. *Int J Prosthodont* 2003 Nov-Dec.16:602-8.
25. Engquist B, Åstrand P, Anzen B, Dahlgren S, Engquist E, Feldmann H, Karlsson U, Nord PG, Sahlholm S, Svårdström P. *Clin Impl Dent Relat Res.* 2005;7(2):95-104  
Simplified methods of implant treatment in edentulous lower jaw: A 3-year follow-up report of a controlled prospective study of one-stage versus two-stage surgery and early loading.
26. Engquist B, Åstrand P, Dahlgren S, et al. Marginal bone reactions to oral implants: A prospective comparative study of Astra Tech and Brånemark System implants. *Clin Oral Implants Res* 2002;13:30-37.
27. Ericsson I, Randow K, Nilner K, Pettersson A. Early loading of Brånemark dental implants: 5-year clinical follow-up study. *Clinical Oral Implant Res* 8:422-426
28. Ericsson I, Nilner K. *Int J Periodontics Restorative Dent.* 2002 Feb;22(1):9-19.  
Early functional loading using Brånemark Dental Implants.
29. Esposito M, Hirsch JM, Lekholm U, Thomsen P. Biological factors contributing to failures of osseointegrated oral implants. (I). Success criteria and epidemiology. *Eur J Oral Sci* 1998 Feb;106(1):527-51.
30. Esposito M, Hirsch JM, Lekholm U, Thomsen P. Biological factors contributing to failures of osseointegrated oral implants. (II). Success criteria and epidemiology. *Eur J Oral Sci* 1998 Feb;106(1):721-764.
31. Friberg B, Nilson H, Olsson M, Palmquist C. Mk II: the self-tapping Branemark implant: 5-year results of a prospective 3-center study. *Clin Oral Implants Res* 1997;8(4):279-285.
32. Friberg B, Sennerby L, Gröndahl K, Bergström C, Bäck T, Lekholm U. On cutting torque measurements during implant installation. A 3-year prospective study. *Clin Impl Dent Relat Res* 1999b:17
33. Friberg B, Jisander S, Widmark G, et al. One year prospective three-center study comparing the outcome of a “soft bone implant” and the standard Brånemark implant. *Clin Impl Dent Relat Res* 2003;5:71-75.
34. Friberg B, Dahlin C, Widmark G, ÖstmanPO, Billström C. One-year results of a prospective multicenter study on Brånemark System implants with a TiUnite surface. *Clin Implant Dent Relat Res.* 2005;7 Suppl 1:570-5.
35. Gardner DM. Platform switching as means to achieving implant esthetics. *NY State Dent J* 2005 Apr;71(3):34-7.
36. Geurs NC, Jeffcoat RL, McGlumphy EA, et al. Influence of implant geometry and surface characteristics on progressive osseointegration. *Int J Oral Maxillofac Implants* 2002;17:811-815.
37. Glantz PO, Rangert B, Svensson A, Stafford GD, Arnvidarson B, Randow K, Linden U, Hulthen J. On clinical loading of osseointegrated implants. A methodological and clinical study. *Clin Oral Implants Res* 1993 Jun;4(2):99-105.

38. Glauser R, Portmann M, Ruhstaller P, Gottlow J, Schärer P. Initial implant stability using different implant designs and surgical techniques. A comparative clinical study using insertion torque and resonance frequency analysis. *Appl Osseointegr Res* 2001;2:6-8.
39. Glauser R, Portmann M, Ruhstaller P, Lundgren AK, Hämmerle C, Gottlow J. Stability measurements of immediately loaded machined and oxidized implants in the posterior maxilla. *Appl Osseointegr Res* 2001;2:27-29.
40. Glauser R, Lundgren AK, Gottlow J, et al. Immediate occlusal loading of Brånemark TiUnite implants placed predominantly in soft bone; 1-year results of a prospective clinical study. *Clin Impl Dent Relat Res* 2003;5:47-56.
41. Gotfredsen K; Nimb L; Hjörting-Hansen E; Jensen J S; Holmén A. (1992) Histomorphometric and removal torque analysis for TiO<sub>2</sub>-blasted titanium implants. An experimental study in dogs. – *Clin Oral Impl Res* 3:77-84.
42. Gotfredsen K, Holm B. Implant-supported mandibular overdentures retained with ball or bar attachments: a randomized prospective 5-year study. *Int J Prosthodont.* 2000 Mar-Apr;13(2):125-30.
43. Gotfredsen K, Karlsson U. A prospective 5-year study of fixed partial prostheses supported by implants with machined and TiO<sub>2</sub>-blasted surface. *J Prosthodont.* 2001;10(1):2-7.
44. Gross M, Abramovich I, Weiss EI. Microleakage at the abutment-implant interface of osseo-integrated implants: a comparative study. *Int J Oral Maxillofac Implants* 1999;14(1):94-100.
45. Gunne J, Rangert B, Glantz PO, Svensson A. Functional loads on freestanding and connected implants in three-unit mandibular prostheses opposing complete dentures: an in vivo study. *Int J Oral Maxillofac Implants* 1997 May-Jun;12(3):335-41.
46. Hallgren C, Sawase T, Örtengren U, Wennerberg A.. Histomorphometric and mechanical evaluation of the bone-tissue response to implants prepared with different orientation of surface topography. *Clin Impl Dent Relat Res* 2001;3:194-203.
47. Hansson S. Implant-abutment interface: biomechanical study of flat top versus conical. *Clin Implant Dent Relat Res* 2000;2(1):33-41.
48. Hansson S. A conical implant-abutment interface at the level of the marginal bone improves the distribution of stresses in the supporting bone. An axisymmetric finite element analysis. *Clin Oral Implants Res* 2003;14:286-293.
49. Hansson S. The Implant neck: smooth or provided with retention elements. A biomechanical approach. *Clin Oral Implants Res.* 1999 Oct;10(5):394-405.
50. Hansson S, Werke M. The implant thread as a retention element in cortical bone: the effect of thread size and thread profile: a finite element study. *J Biomech,* 2003 Sep;36(9):1247-58.
51. Hellem S, Karlsson U, Almfeldt I, Brunell G, Hamp SE, Astrand P. Nonsubmerged implants in the treatment of the edentulous lower jaw: a 5-year prospective longitudinal study of ITI hollow screws. *Clin Implant Dent Relat Res.* 2001;3(1):20-29.
52. Henry P J, Laney W R, Jemt T, Harris D, Krogh P H J, Polizzi G, Zarb G A, Herrmann I. Osseointegrated implants for single-tooth replacement: A prospective 5-year multicenter study. *Int J Oral Maxillofac Implants.* 1996; 11(4):450-455.
53. Herrmann I, Lekholm U, Holm S, Kultje C. Prognostic factors in dental implant treatment. *Int J Oral Maxillofac Implants.* 2005 Mar-Apr;20(2):220-30.
54. Ivanoff C-J, Hallgren C, Widmark G, Sennerby L, Wennerberg A. Histologic evaluation of the bone integration of TiO<sub>2</sub> blasted and turned titanium microimplants in humans.. *Clin Oral Implant Res.* 12, 2001;128-134.
55. Ivanoff C-J, Widmark G, Johansson C, Wennerberg A. Histologic Evaluation of bone response to oxidized and turned titanium micro-implants in human jawbone. *Int J Oral Maxillofac Implants* 2003;18:341-348.
56. Jeffcoat RL, McGlumphy EA, Reddy MS, et al. A comparison of hydroxyapatite-coated threaded, HA-coated cylindrical, and titanium threaded endosseous dental implants. *Int J Oral Maxillofac Implants* 2003;18:406-410.
57. Jemt T, Lekholm U. Oral implant treatment in posterior partially edentulous jaws: A 5-year follow-up report. *Int J Oral Maxillofac Implants* 1993;8:635-640.
58. Jemt T, Lekholm U. Implant treatment in edentulous maxillae: A 5-year follow-up report on patients with different degrees of jaw resorption. *Int J Oral Maxillofac Implants* 1995;10:303-311.

59. Jemt T, Book K. Prosthesis misfit and marginal bone loss in edentulous implant patients. *Int J Oral Maxillofac Implants* 1996 Sep-Oct;11(5):620-5.
60. Jemt T, Chai J, Harnett J, Heath M R, Hutton J E, Johns R B, McKenna S, McNamara D C, van Steenberghe D, Taylor R, Watson R M, Herrmann I. A 5-year prospective multicenter follow-up report on overdentures supported by osseointegrated implants. *Int J Oral Maxillofac Implants.* 1996;11(3):291-298.
61. Jemt T, Lekholm U, Johansson CB. Bone response to implant-supported frameworks with differing degrees of misfit preload: in vivo study in rabbits. *Clin Implant Dent Relat Res* 2000;2(3):129-37.
62. Jokstad A, Braegger U, Brunski J, Carr A, Naert I, Wennerberg A. Quality of dental implants. *International Dental Journal* (2003) Vol.53/No.6.
63. Karlsson U, Gotfredsen K, Olsson C. A 2-year report on maxillary and mandibular fixed partial dentures supported by Astra Tech dental implants. A comparison of two implants with different surface textures. *Clin Oral Implants Res* 1998;9:235-242.
64. Keller W, Bragger U, Mombelli A. Peri-implant microflora of implants with cemented and screw retained suprastructures. *Clin Oral Implants Res* 1998;9(4):209-217.
65. Kempainen P, Eskola S, Ylipaavalmi PA. A comparative prospective clinical study of two single-tooth implants: A preliminary report of 102 implants. *J Prosthet Dent* 1997;77:382-387.
66. Kinsel R P, Lamb R E. Tissue-directed placement of dental implants in the esthetic zone for long-term biologic synergy: A clinical report. *Int J Oral Maxillofac Implants* 2005;20:913-922.
67. Kirketerp P, Andersen JB, Urde G. Replacement of extracted anterior teeth by immediately loaded Replace Select HA-coated implants. A one-year follow-up of 35 patients. *Applied Osseointegration Research* 2002;1(3):40-42.
68. Lazzara R, Siddiqui AA, Binon P, Feldman SA, Weiner R, Phillips R, Gonshor A. Retrospective multicenter analysis of 31<sup>®</sup> endosseous dental implants placed over a five-year period. *Clin Oral Implants Res.* 1996;7(1):73-83.
69. Lazzara RJ, Porter SS, Testori T, Galante J, Zetterqvist L. A prospective multicenter study evaluating loading of osseotite implants two months after placement: one-year results. *J Esthet Dent* 1998;10(6):280-289.
70. Lekholm U, van Steenberghe D, Herrmann I, Bolender C, Folmer T, Gunne J, Henry P, Higuchi K, Laney W R, Lindén U. Osseointegrated implants in the treatment of partially edentulous jaws. A prospective 5-year multicenter study. *Int J Oral Maxillofac Implants.* 1994;9:627-635.
71. Lekholm U, Gunne J, Henry P, Higuchi K, Linden U, Bergstrom C, van Steenberghe D. Survival of the Branemark implant in partially edentulous jaws: a 10-year prospective multicenter study. *Int J Oral Maxillofac Implants.* 1999;14(5):639-645.
72. Listgarten MA, Lang HP, Schroeder HE, Schroeder A. Periodontal tissues and their counterparts around endosseous implants. *Clin Oral Implants Res* 1991;2:1-19.
73. Meijer HJ, Raghoobar GM, Van 't Hof MA, Visser A, Geertman ME, Van Oort RP. A controlled clinical trial of implant-retained mandibular overdentures; five-years' results of clinical aspects and aftercare of IMZ implants and Branemark implants. *Clin Oral Implants Res.* 2000;11(5):441-447.
74. Moberg LE, Kondell PA, Sagulin GB, Bolin A, Heimdahl A, Gynther GW. Branemark System and ITI Dental Implant System for treatment of mandibular edentulism. A comparative randomized study: 3-year follow-up. *Clin Oral Implants Res.* 2001 OCT;12(5):450-61.
75. Naert IE, Koutsikakis G, Quirynen M, et al. Biologic outcome of implant-supported restorations in treatment of partial edentulism. Part I: A longitudinal clinical evaluation. *Clin Oral Implants Res* 2002;13:381-389.
76. Naert IE, Koutsikakis G, Duyck JA, et al. Biologic outcome of implant-supported restorations in treatment of partial edentulism. Part 2: A longitudinal clinical evaluation. *Clin Oral Implants Res* 2002;13:390-395.
77. Norton MR. An in vitro evaluation of the strength of an internal conical interface compared to a butt joint interface in implant design. *Clin Oral Implants Res* 1997 Aug;8(4):290-298.
78. Norton MR. Marginal bone levels at single tooth implants with a conical fixture design. The influence of surface macro- and microstructure. *Clin Oral Implants Res* 1998;9(2):91-99.

79. Oh T-J, Yoon J, Misch CE, Wang H\_L. The cause of early implant bone loss: Myth or science?. *J Periodontol* 2002;73:322-333.
80. Olsson M, Urde G, Andersen JB, Sennerby L. Early loading of maxillary fixed cross-arch dental prostheses supported by six or eight oxidized titanium implants: Results after 1 year of loading, case series. *Clin Impl Dent Relat Res* 2003;5:81-87.
81. O'Sullivan D, Sennerby L, Meredith N. Measurements comparing the initial stability of five designs of dental implants: a human cadaver study. *Clin Implant Dent Relat Res* 2000;2(2):85-92.
82. Palmer RM, Palmer PJ, Smith BJ. A 5-year prospective study of Astra single tooth implants. *Clin Oral Implants Res*. 2000 Apr;11(2):179-82.
83. Quirynen M, Naert I, van Steenberghe D. Fixture design and overload influence marginal bone loss and fixture success in the Brånemark system. *Clin Oral Impl Res* 1992;3:110-111.
84. Quirynen M, Bollen CM, Papaioannou W, et al. The influence of titanium abutment surface roughness on plaque accumulation and gingivitis: A short-term observation. *Int J Oral Maxillofac Implants* 1996;11:169-178.
85. Perignon D, Taittinger P. Implant generated benefits. 1990;75-150.
86. Rangert B, Krogh PH, Langer B, Van Roekel N. Bending overload and implant fracture: a retrospective clinical analysis. *Int J Oral Maxillofac Implants* 1995 May-Jun;10(3):326-34.
87. Rangert BR, Sullivan RM, Jemt TM. Load factor control for implants in the posterior partially edentulous segment. *Int J Oral Maxillofac Implants* 1997 May-Jun;12(3):360-70.
88. Rangert B, Sennerby L, Meredith N, Brunski J. Design, maintenance and biomechanical considerations in implant placement. *Dent Update* 1997 Dec;24(10):416-20.
89. Rocci A, Martignoni M, Burgos PM, Gottlow J. Immediate loading of Brånemark system TiUnite and machined-surface implants in the posterior mandible: A randomized open-ended clinical trial. *Clin Implant Dent Relat Res* 2003;5:57-63.
90. Rocci A, Martignoni M, Burgos PM, Gottlow J, Sennerby L. Histology of retrieved immediately and early loaded oxidized Implants: Light microscopic observations after 5 to 9 months of loading in the posterior mandible. *Clin Impl Dent Relat Res* 2003;5:88-98.
91. Rutar A, Lang NP, Buser D, Burgin W, Mombelli A. Retrospective assessment of clinical and microbiological factors affecting periimplant tissue conditions. *Clin Oral Implants Res*. 2001 Jun;12(3):189-95.
92. Salata L, Rasmusson L, Novaes A, Papalexiou V, Sennerby L. The influence of anodic oxidation on implant integration and stability in the dog mandible. *Appl Osseointegration Res* 2002;3:1:32-34
93. Sahiwal IG, Woody RD, Benson BW, et al. Macro design morphology of endosseous dental implants. *J Prosthet Dent* 2002;87:543-551
94. Scheller H, Urgell JP, Kultje C, Klineberg I, Goldberg PV, Stevenson-Moore P, Alonso JM, Schaller M, Corria RM, Engquist B, Toreskog S, Kastenbaum F, Smith CR. A 5-year multicenter study on implant-supported single crown restorations. *Int J Oral Maxillofac Implants*. 1998;13(2):212-218.
95. Schnitman PA, Wohrle PS, Rubenstein JE, DaSilva JD, Wang NH. *Int J Oral Maxillofac Implants*. Jul-Aug;12(4):495-503. Ten-year results for Brånemark Implants immediately loaded with fixed prostheses at implant placement.
96. Sennerby L, Roos J. Surgical determinants of clinical success of osseointegrated oral implants: A review of the literature. *Int J Prosthodont* 1998;11:408-420
97. Sennerby L, Persson LG, Berglundh T, Wennerberg A, Lindhe L. Implant stability during initiation and resolution of experimental periimplantitis: an experimental study in the dog. *Clin Implant Dent Relat Res*. 2005;7(3):136-40.
98. Sul YT, Johansson CB, Jeong Y, Albrektsson T. The electrochemical oxide growth behaviour on titanium in acid and alkaline electrolytes. *Med Eng Phys*. 2001 Jun;23(5):329-46.
99. Sul YT. On the bone response to oxidized titanium implants: The role of microporous structure and chemical composition of the surface oxide in enhanced osseointegration. Thesis, University of Göteborg. – ISBN 91-628-5221-3.
100. Sul YT, Johansson CB, Roser K, Albrektsson T. Qualitative and quantitative observations of bone tissue reactions to anodised implants. *Biomaterials*. 2002 Apr;23(8):1809-17.
101. Sul YT, Johansson CB, Petronis S, Krozer A, Jeong Y, Wennerberg A, Albrektsson T. Characteristics of the surface oxides on turned and electrochemically oxidized pure titanium implants up to dielectric breakdown: the oxide thickness, micropore configurations, surface roughness, crystal structure and chemical composition. *Biomaterials*. 2002 Jan;23(2):491-501.
102. Tawse-Smith A, Payne AG, Kumara R, Thomson WM. Early load of unsplinted implants supporting mandibular over-dentures using one-stage operative procedure with two different implant systems: A 2-year report. *Clin Implant Dent Relat Res* 2002;4:33-42.
103. van Steenberghe D, Klinge B, Linden U, Quirynen M, Herrmann I, Garpland C. Periodontal indices around natural and titanium abutments: a longitudinal multicenter study. *J Periodontol* 1993 Jun;64(6):538-41.
104. van Steenberghe D, De Mars G, Quirynen M, Jacobs R, Naert I. A prospective split-mouth comparative study of two screw-shaped self-tapping pure titanium implant systems. *Clin Oral Implants Res* 2000;11(3):202-209.
105. Weigl P. New prosthetic restorative features of Ankylos® implant system. *J Oral implantol*. 2004;30(3):178-88.
106. Wennerberg A, Albrektsson T, Andersson B, Kroll JJ. A histomorphometric and removal torque study of screw-shaped titanium implants with three different surface topographies. *Clin Oral Impl Res* 1995;6:24-30.
107. Wennerberg A. (1996) On surface roughness and implant incorporation, Thesis, University of Göteborg. – ISBN 91-628-1940-2.
108. Wennerberg A, Albrektsson T. Suggested guidelines for the topographic evaluation of implant surfaces. *Int J Oral Maxillofac Implants*. 2000;15(3):331-344.
109. Wennerberg A, Hallgren C, Johansson C, Danelli S. A histomorphometric evaluation of screw-shaped implants each prepared with two surface roughness. *Clin Oral Implants Res*. 1998 Feb;9(1):11-9.
110. Åstrand P, Engquist B, Dahlgren S, Engquist E, Fieldmann H, Gröndahl K. Astra Tech and Brånemark implants; A prospective 5-year comparative study. Results after one year. *Clin Impl Dent Relat Res* 1999;1:1726.
111. Åstrand P, Engquist B, Anzen B, Bergendal T, Hallman M, Karlsson U, Kvint S, Runderantz T. *Clin Implant Dent Relat Res*. 2002;4(3):115-27 Nonsubmerged and submerged implants in treatment of the partially edentulous maxilla.
112. Östman PO, Hellman M, Wendelhag I, Sennerby L. Resonance frequency analysis measurements of implants at placement surgery. *Int J Prosthodont*. 2006 Jan-Feb; 19(1):77-83.

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